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## Skeletal muscle oxidative function in vivo and ex vivo in athletes with marked hypertrophy from resistance training

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**Salvadego D, Domenis R, Lazzar S, Porcelli S, Rittweger J, Rizzo G, Mavelli I, Šimunič B, Pišot R, Grassi B.** Skeletal muscle oxidative function in vivo and ex vivo in athletes with marked hypertrophy from resistance training. *J Appl Physiol* 114: 1527–1535, 2013. First published March 21, 2013; doi:10.1152/jappphysiol.00883.2012.—Oxidative function during exercise was evaluated in 11 young athletes with marked skeletal muscle hypertrophy induced by long-term resistance training (RTA; body mass  $102.6 \pm 7.3$  kg, mean  $\pm$  SD) and 11 controls (CTRL; body mass  $77.8 \pm 6.0$  kg). Pulmonary  $O_2$  uptake ( $\dot{V}O_2$ ) and vastus lateralis muscle fractional  $O_2$  extraction (by near-infrared spectroscopy) were determined during an incremental cycle ergometer (CE) and one-leg knee-extension (KE) exercise. Mitochondrial respiration was evaluated ex vivo by high-resolution respirometry in permeabilized vastus lateralis fibers obtained by biopsy. Quadriceps femoris muscle cross-sectional area, volume (determined by magnetic resonance imaging), and strength were greater in RTA vs. CTRL (by  $\sim 40\%$ ,  $\sim 33\%$ , and  $\sim 20\%$ , respectively).  $\dot{V}O_{2peak}$  during CE was higher in RTA vs. CTRL ( $4.05 \pm 0.64$  vs.  $3.56 \pm 0.30$  l/min); no difference between groups was observed during KE. The  $O_2$  cost of CE exercise was not different between groups. When divided per muscle mass (for CE) or quadriceps muscle mass (for KE),  $\dot{V}O_2$  peak was lower (by 15–20%) in RTA vs. CTRL. Vastus lateralis fractional  $O_2$  extraction was lower in RTA vs. CTRL at all work rates, during both CE and KE. RTA had higher ADP-stimulated mitochondrial respiration ( $56.7 \pm 23.7$  pmol  $O_2 \cdot s^{-1} \cdot mg^{-1}$  ww) vs. CTRL ( $35.7 \pm 10.2$  pmol  $O_2 \cdot s^{-1} \cdot mg^{-1}$  ww) and a tighter coupling of oxidative phosphorylation. In RTA, the greater muscle mass and maximal force and the enhanced mitochondrial respiration seem to compensate for the hypertrophy-induced impaired peripheral  $O_2$  diffusion. The net results are an enhanced whole body oxidative function at peak exercise and unchanged efficiency and  $O_2$  cost at submaximal exercise, despite a much greater body mass.

skeletal muscle hypertrophy; mitochondrial respiration; oxidative metabolism during exercise

RESISTANCE TRAINING PROGRAMS have been developed with the aim of improving variables of muscle function such as strength, power, speed, local muscular endurance, coordination, and flexibility (21). Resistance training is now considered an important part of training and rehabilitation programs for healthy subjects and for various types of patients, such as cardiac patients (45), patients with pulmonary diseases (10), patients undergoing prolonged bed-rest periods (2), or elderly

subjects (28). In these populations, the combination of resistance training with the more conventional endurance exercise improves the patients' outcomes and quality of life (45).

An increase in the cross-sectional area of skeletal muscle fibers and a shift of fiber-type distribution toward type 2 fibers are typical adaptations induced by resistance training; these adaptations enhance the muscle force-generating potential (12) but could represent an impairment to skeletal muscle oxidative metabolism. On the other hand, muscles with higher maximal force would need to recruit a lower number of motor units, and therefore more oxidative (and more efficient) muscle fibers (20, 26). According to other authors, strength training may increase skeletal muscle efficiency (4) and enhance skeletal muscle "metabolic stability" (50). Other studies reported, after resistance training, unchanged values of maximal  $O_2$  uptake ( $\dot{V}O_2$ ) (6), as well as unchanged (19) or lower (42, 43) mitochondrial volume density, oxidative enzyme activity, and capillary density in the hypertrophic muscles. Thus the specific effects of resistance training, with the related changes in muscle phenotype, on oxidative metabolism appear difficult to reconcile in a unifying scenario. The aim of the present study was to determine whether increases in muscle mass induced by chronic resistance training are associated, in humans, with alterations in skeletal muscle oxidative function and aerobic performance. Experiments were carried out on a group of resistance-trained athletes (RTA), in whom muscle adaptations to resistance exercise are expected to be particularly marked. An integrative approach was applied by analyzing oxidative metabolism at different levels, spanning from pulmonary gas exchange to skeletal muscle function and mitochondrial respiration. Oxidative function was assessed in vivo during incremental cycle ergometer (CE) exercise and dynamic knee extension (KE) exercise with one leg (3). During KE, the recruitment of a relatively small muscle mass, i.e., the quadriceps femoris of one leg, significantly reduces constraints to oxidative function deriving from cardiovascular  $O_2$  delivery, thereby allowing a more direct assessment of quadriceps muscle oxidative capacity in vivo. The intrinsic properties of mitochondria were assessed ex vivo in permeabilized muscle fibers obtained by biopsy by high-resolution respirometry (36).

We hypothesized, in RTA vs. control subjects (CTRL), an impaired skeletal muscle oxidative function in vivo and an impaired mitochondrial respiratory function ex vivo.

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## MATERIALS AND METHODS

### Subjects

We evaluated 11 male RTA [age,  $25.4 \pm 6.1$  (means  $\pm$  SD) yr; body mass (BM),  $102.6 \pm 7.3$  kg; height,  $1.84 \pm 0.04$  m; body mass index (BMI),  $30.1 \pm 2.6$  kg/m<sup>2</sup>], who had been following for at least 5 yr resistance-training programs specifically designed to increase quadriceps muscle strength and power, and 11 physically active CTRL (age,  $25.4 \pm 3.8$  yr; BM,  $77.8 \pm 6.0$  kg; height,  $1.81 \pm 0.05$  m; BMI,  $23.8 \pm 2.2$  kg/m<sup>2</sup>). A thigh circumference above 60 cm (with thigh fat thickness below 10 mm) was taken as a criterion for including subjects in the RTA group. A diary of the training regimen and physical activity, focused on the 8 wk preceding the evaluation, was collected. RTA practiced sport activities such as American football (tackle position), track and field (throwing), and weight lifting for an average of  $487 \pm 204$  min/wk. Most of them took part at national-level competitions and championships. In their training sessions, RTA included standard protocols of resistance exercise targeting all major upper body and lower body muscle groups. The RTA training regimen could be categorized as high-intensity and low-volume resistance exercise training (21). The RTA subjects also practiced aerobic exercise such as running and cycling for  $\sim 127 \pm 150$  min/wk. CTRL practiced running and cycling for  $\sim 153 \pm 133$  min/wk and sport activities such as tennis, handball, or gym activities for  $102 \pm 143$  min/wk, respectively, essentially for recreational purposes. They did not follow any resistance training program or any other specific training schedule.

Careful medical and pharmacological histories were collected. RTA and CTRL were not affected by any disease and were not taking any drug at the time of the study. RTA did not report any drug misuse to support their training. Participants were informed about the aims and methods of the investigation and gave their written, informed consent. The experiments were carried out at the Valdoltra Orthopaedic Hospital of Ankaran, Slovenia. All procedures conformed to the declaration of Helsinki (2000) and were approved by the Slovenian National Medical Ethics Committee.

All tests were conducted under close medical supervision and followed standard safety procedures, and the subjects were continuously monitored by 12-lead electrocardiography (ECG).

### Exercise Protocols

Incremental exercise protocols were carried out by utilizing a mechanically braked CE (Monark Ergonomic 839E) and a custom-built KE ergometer (modified Monark cycle ergometer), as originally described by Andersen et al. (3). The exercise protocols were conducted in random order during different experimental sessions separated by a 24-h recovery period.

During CE, subjects performed an initial 4 min of pedalling at 80 W; thereafter, 20-W increments were imposed every minute until voluntary exhaustion. Pedalling frequency was kept at  $\sim 60$  rpm, as imposed by a metronome. During KE, subjects were constrained on an adjustable seat by a safety belt, which anchored the angle of the hip at  $\sim 90^\circ$ . Subjects pushed on a padded bar attached to a lever arm connected to the crank of the cycle ergometer, which allowed a knee extension between  $\sim 90^\circ$  and  $\sim 170^\circ$ . This type of exercise confines muscle contractile activity to the quadriceps femoris muscle of one leg, which is activated during the extension phase. The return of the leg to the starting position is brought about passively by the momentum of the flywheel of the ergometer (see Ref. 37 for details). Before data collection, each subject was familiarized with the setup environment and the exercise protocol by short preliminary practice runs. After an initial 3 min of unloaded KE exercise, an incremental test was performed. Work rate increments were imposed every minute to allow the subjects to reach exhaustion in  $\sim 10$  min. Work rate was applied by adjusting the tension of a strap around the ergometer flywheel, as in a mechanically braked cycle ergometer. Throughout

the test, the active KE and passive knee flexion cycle was carried out  $\sim 40$  times per min, as imposed by a metronome. During each cycle (total duration of 1.5 s), KE lasted  $\sim 1$  s. In other words, muscle contraction corresponded to  $\sim 65\%$  of the duty cycle.

All the exercises were conducted up to the limit of tolerance. The latter was defined as the inability to maintain the imposed work rate at the required frequency despite vigorous encouragement by the operators. Mean values of cardiovascular, ventilatory, gas exchange, and muscle oxygenation variables (see below) were calculated during the last 20 s of each work rate; values obtained during the exhausting work rate were considered "peak" values.

### Measurements

**Anthropometry.** Fat-free mass (FFM) and total skeletal muscle mass were assessed by bioelectric impedance analysis (BIA) performed by a tetrapolar device (Human IM, Dietosystem, Italy), in accordance with the conventional standard technique (25).

**Anatomical cross-sectional area, muscle volumes, and muscle force.** Anatomical cross-sectional area (CSA) of right thigh muscles and of the right quadriceps were measured from turbo spin-echo, T1-weighted, magnetic resonance images (MRI) obtained with 1.5 T (Magnetom Avanto; Siemens Medical Solution, Erlangen, Germany). On each MRI slice, contours corresponding to the thigh muscles and quadriceps were delineated by an expert of MRI imaging, using the image processing tools available in the commercial software package AMIRA (version 4.1, Mercury Computer System, Chelmsford, MA). The volumes of thigh muscles and quadriceps were then derived as the geometrical volumes included in these contours.

Before the incremental tests, subjects performed two maximal voluntary isometric contractions (MVC) of the knee extensors of the right leg at a  $110^\circ$  knee angle. Force was measured by an electrical transducer (TSD121C, BIOPAC Systems) implemented on a custom-built chair for isometric contractions of knee extensor and flexor muscle groups. Force was sampled at a frequency of 1 kHz (MP100, BIOPAC Systems).

**Measurements during the incremental tests.** Time to exhaustion was taken as an index of performance. Pulmonary ventilation ( $\dot{V}_E$ ), tidal volume ( $V_T$ ), respiratory frequency ( $f$ ), O<sub>2</sub> uptake ( $\dot{V}_{O_2}$ ), and CO<sub>2</sub> output ( $\dot{V}_{CO_2}$ ) were determined on a breath-by-breath basis by means of a metabolic unit (Quark b<sup>2</sup>, Cosmed, Italy). Expiratory flow measurements were performed by a turbine flow meter calibrated before each experiment by a 3-liter syringe at three different flow rates. Calibration of O<sub>2</sub> and CO<sub>2</sub> analyzers was performed before each experiment by utilizing gas mixtures of known composition. The gas exchange ratio (R) was calculated as  $\dot{V}_{CO_2}/\dot{V}_{O_2}$ . The gas exchange threshold (GET) was determined by the V-slope method (5). All the data related to GET were expressed as a percentage of  $\dot{V}_{O_{2peak}}$ .

During KE, a biphasic pattern in the  $\dot{V}_{O_2}$  vs. work rate relationship was observed (see Ref. 34). During CE,  $\dot{V}_{O_2}$  and  $\dot{V}_{O_{2peak}}$  values were expressed as liters per minute and normalized per unit of whole body muscle mass ( $\text{ml} \cdot \text{min}^{-1} \cdot \text{kg}^{-1}$ ), whereas, during KE,  $\dot{V}_{O_2}$  and  $\dot{V}_{O_{2peak}}$  values were expressed as liters per minute and normalized as milliliters per minute per 100 g of quadriceps muscle mass (QM). The latter was calculated on the basis of quadriceps muscle volume (see above), after assuming a standard value for skeletal muscle density of 1.060 kg/liter (27).

Heart rate (HR) was determined by ECG. Stroke volume (SV) was estimated beat by beat by impedance cardiography (Physio Flow, Manatec, Paris, France) (33). The accuracy of this device has been previously evaluated during incremental exercise in healthy subjects against the direct Fick method (33); in that study, the correlation coefficient between the two methods was  $r = 0.946$  ( $P < 0.01$ ), and the mean difference was equal to  $-2.78 \pm 12.33\%$  (2 SD). Overall, the accuracy of this method can be considered "acceptable" for the purpose of the study, which is to demonstrate that the cardiac involvement during KE was not "maximal" also at peak exercise (as

confirmed also from HR measurements). Cardiac output ( $\dot{Q}$ ) was calculated as  $HR \times SV$ . Cardiac index (CI;  $\dot{Q}/\text{body surface}$ ) was also determined to take into account the difference in body size between RTA and CTRL.

Oxygenation changes in vastus lateralis muscle were evaluated by near-infrared spectroscopy (NIRS) (7, 13). Reliability of tissue oxygenation indexes obtained by NIRS, evaluated by the intraclass correlation coefficient for repeated measurements on the same subject during different days, was found to be very high for skeletal muscle (41). NIRS measurements in muscle tissue have been shown to be well correlated with local venous  $O_2$  saturation (48). A portable NIR continuous-wave photometer (PortaMon, Artinis, The Netherlands) was utilized. Specific details on the method can be found in recent papers by our group (32, 37). The instrument measures micromolar ( $\mu\text{M}$ ) changes in oxygenated hemoglobin (Hb) + myoglobin (Mb) concentrations [ $\Delta[\text{oxy}(\text{Hb}+\text{Mb})]$ ], and in deoxygenated [Hb + Mb] [ $\Delta[\text{deoxy}(\text{Hb}+\text{Mb})]$ ], with respect to an initial value arbitrarily set equal to zero and obtained during the resting condition preceding the test.  $\Delta[\text{deoxy}(\text{Hb}+\text{Mb})]$  is relatively insensitive to changes in blood volume and has been considered an estimate of skeletal muscle fractional  $O_2$  extraction (ratio between  $O_2$  consumption and  $O_2$  delivery) (15, 18). A "physiological calibration" of  $\Delta[\text{deoxy}(\text{Hb}+\text{Mb})]$  values was performed by obtaining a transient ischemia of the limb after the exercise period: data obtained during exercise were expressed as a percentage of the values of maximal muscle deoxygenation obtained by pressure cuff inflation (at 300–350 mmHg), carried out at the inguinal crease of the thigh for a few minutes until  $\Delta[\text{deoxy}(\text{Hb}+\text{Mb})]$  increase reached a plateau (18).  $\Delta[\text{deoxy}(\text{Hb}+\text{Mb})]$  kinetics during the incremental tests were fitted by a sigmoid function, as proposed by Ferreira et al. (14).

**Skeletal muscle biopsy and high-resolution respirometry.** Muscle samples were obtained from the vastus lateralis muscle of the left limb by percutaneous biopsy, which was taken, for all subjects, 5 h after the last incremental test. Biopsy was done after anesthesia of the skin, the subcutaneous fat tissue, and the muscle fascia with 2 ml of lidocaine (2%). A small skin incision was then made to penetrate skin and fascia, and the tissue sample was harvested with a purpose-built rongeur (Zepf Instruments, Tuttlingen, Germany). The muscle samples were divided into two portions. One portion (~10 mg wet wt) was immediately frozen in liquid nitrogen and stored at  $-80^\circ\text{C}$  until enzymatic determination of citrate synthase (CS) activity. The other portion (~10 mg wet wt) was used to measure mitochondrial respiration *ex vivo* and was immediately placed in an ice-cold relaxing solution containing (in mM) 10 EGTA-calcium buffer (free  $\text{Ca}^{2+}$  concentration 100 nmol/l), 20 imidazole, 20 taurine, 50  $\text{K}^+/4$  morpholinoethanesulfonic acid (K-MES), 0.5 dithiothreitol (DTT), 6.56  $\text{MgCl}_2$ , 5.77 ATP, and 15 phosphocreatine, pH 7.1.

The fiber bundles were separated with sharp-ended needles, leaving only small areas of contact, and were incubated in 5 ml of the above solution ( $4^\circ\text{C}$ ), containing 50  $\mu\text{g}/\text{ml}$  saponin for 30 min with continuous gentle stirring to ensure complete permeabilization. After being rinsed twice for 10 min in a respiration medium (MiRO5, Oroboros, Innsbruck, Austria; 0.5 mM EGTA, 60 mM potassium lactobionate, 3 mM  $\text{MgCl}_2 \cdot 6\text{H}_2\text{O}$ , 20 mM taurine, 10 mM  $\text{KH}_2\text{PO}_4$ , 20 mM HEPES, 110 mM sucrose, and 1 g/l BSA, pH 7.1), permeabilized fibers were measured for wet weight and immediately transferred into a respirometer (Oxygraph-2k; Oroboros Instruments, Innsbruck, Austria) for the analysis.

Mitochondrial respiratory function was evaluated by measuring  $O_2$  consumption polarographically by high-resolution respirometry (17, 29). Data were digitally recorded using DatLab4 software (Oroboros Instruments). The instrumentation allows for  $O_2$  consumption measurements with small amounts of sample in closed respiration chambers containing 3 ml of air-saturated respiration medium at  $30^\circ\text{C}$ ; 3–5 mg of muscle fibers were used for the analysis. Standardized instrumental and chemical calibrations were performed to correct for back-diffusion of  $O_2$  into the chamber from the various components, leak from the exterior,  $O_2$  consumption by the chemical medium, and

sensor  $O_2$  consumption (29). The  $O_2$  concentration in the chamber was maintained between 250 and 400  $\mu\text{M}$  to avoid  $O_2$  limitation of respiration. Intermittent reoxygenation steps were performed during the experiments by adding a 200 mM hydrogen peroxide solution into the medium containing catalase (29). A substrate-uncoupler-inhibitor-titration protocol with a substrate combination that matches physiological intracellular conditions was applied (17). Non-phosphorylating resting mitochondrial respiration was measured in the presence of malate (4 mM), glutamate (10 mM), and succinate (10 mM), without ADP, so that  $O_2$  consumption was mainly driven by the back leakage of protons through the inner mitochondrial membrane ("leak" respiration). ADP-stimulated mitochondrial respiration (*state 3* respiration) was measured after the subsequent addition of ADP (2.5 mM) as phosphate acceptor with malate, glutamate, and succinate as substrates. The addition of cytochrome *c* (10  $\mu\text{M}$ ) had no additive effects on respiration, with minor increases of ~2%, thereby confirming the integrity of the outer mitochondrial membrane. We also examined electron transport system capacity by stepwise addition of the chemical uncoupler protonophore carbonyl cyanide-*p*-trifluoromethoxyphenylhydrazone (FCCP) to optimum concentration (1.25  $\mu\text{M}$ ). Rotenone (1  $\mu\text{M}$ ) and antimycin A (2.5  $\mu\text{M}$ ) were added to inhibit complexes I and III, providing a measure of residual  $O_2$  consumption, indicative of non-mitochondrial  $O_2$  consumption. Mitochondrial respiration was then corrected for  $O_2$  flux due to the residual  $O_2$  consumption. The respiratory acceptor control ratio (RCR), taken as an index of coupling between electron transfer and phosphorylation, was obtained by dividing *state 3* respiration by leak respiration.

CS activity was determined in frozen fiber bundles (~5 mg wet wt), which were homogenized in buffer (2.5% wt/vol) containing 250 mM sucrose, 40 mM KCl, 2 mM EGTA, 20 mM Tris-HCl (pH 7.4) and supplemented with 0.1% Triton X-100. CS activity was assayed according to Srere (40) by spectrophotometric methods (Lambda 14 Spectrometer; Perkin Elmer) and was expressed as micromoles of substrate per minute per gram of total protein content. Protein content was estimated by Bradford assay (8).

#### Statistical Analysis

Results were expressed as means  $\pm$  SD. Statistical significance of differences between groups (RTA vs. CTRL) was checked by two-tailed Student's *t*-test for unpaired data. Bonferroni correction was used for multiple comparisons. The level of significance was set at  $P < 0.05$ . Statistical analyses were carried out with software packages (GraphPad Prism 4.0, GraphPad Software; SPSS, Statistical Package Social Sciences, 13.0.1).

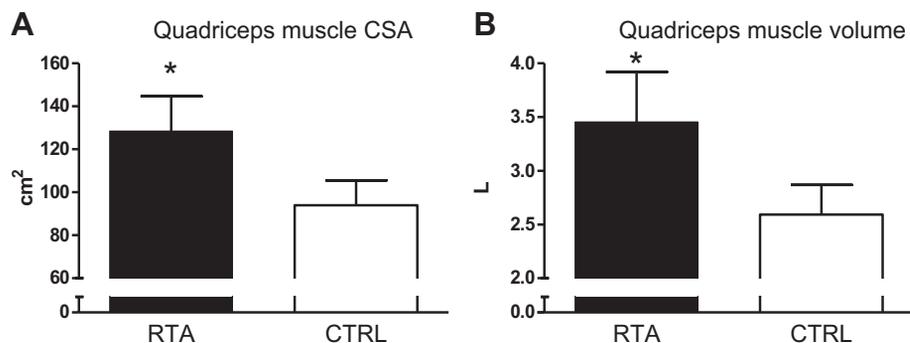
## RESULTS

Values of the anatomical cross-sectional area (CSA) of quadriceps muscle, calculated at 50% femur length, are shown in Fig. 1A. As expected on the basis of the selective inclusion criteria of the study, CSA in RTA was significantly greater (by 37%) than in CTRL. Also, the volume of the quadriceps was significantly greater (by 33%) in RTA vs. CTRL (Fig. 1B). Values of BM, BMI, fat-free mass, skeletal muscle mass, and quadriceps muscle mass are reported in Table 1. For all variables, values in RTA were significantly (by ~30%) greater in RTA vs. CTRL. Also, the percentage of body fat was slightly but significantly greater in RTA vs. CTRL.

The mean force exerted by the knee extensors during MVC was significantly higher (by 18%;  $P = 0.026$ ) in RTA ( $998 \pm 163$  N) vs. CTRL ( $811 \pm 188$  N). Once normalized per unit of CSA, values did not differ between groups ( $7.9 \pm 0.8$  N/cm<sup>2</sup> in RTA vs.  $8.7 \pm 1.9$  N/cm<sup>2</sup> in CTRL).

Peak values of the main ventilatory and gas-exchange variables determined at the limit of tolerance during CE and KE are

Fig. 1. Anatomical cross-sectional area (CSA) of the quadriceps muscle, obtained by magnetic resonance imaging at 50% femur length (A) and quadriceps muscle volume (B) in resistance-trained athletes (RTA) and control subjects (CTRL). Values are means  $\pm$  SD. \*Significant difference vs. control subjects (CTRL;  $P < 0.05$ ). See text for further details.



presented in Table 2. Ventilatory variables were not different in the two groups, both during CE and KE, with the exception of a higher VT peak in RTA during CE. When expressed in liters per minute,  $\dot{V}O_{2peak}$  was higher in RTA vs. CTRL during CE; no significant difference was observed during KE. When  $\dot{V}O_{2peak}$  was expressed per unit of body mass or body muscle mass (for CE) and per unit of quadriceps muscle mass (for KE), values were significantly lower (by  $\sim 15$ – $20\%$ ) in RTA vs. CTRL. Peak work rate was slightly but not significantly higher during CE in RTA vs. CTRL; time to exhaustion values were not different in the two groups during either CE or KE. R peak values were higher than 1.1 in both groups during both types of exercise. Peak values of HR,  $\dot{Q}$ , and CI were similar between RTA and CTRL during either KE or CE (Table 2). As expected, in both groups, peak values of cardiovascular variables obtained in KE were significantly lower than in CE.

Pulmonary  $\dot{V}O_2$  values (ml/min) are plotted as a function of work rate in Fig. 2 during CE (left) and KE (right). To obtain these figures, individual  $\dot{V}O_2$  values were grouped for discrete work rate intervals, which were determined to have, in each interval, each subject represented by one data point. When the subject had more than one “original” data point in the interval, mean individual values were calculated, both for the  $x$  and the  $y$  variables, and were taken in consideration to obtain the figure.

As for CE, mean  $\pm$  SD values of the intercepts and of the slopes of the individual linear regression lines (shown in the figure legend) were not significantly different in RTA vs. CTRL. The mean slopes of the individual regression lines were  $10.6 \pm 0.9$  ml $\cdot$ min<sup>-1</sup> $\cdot$ W<sup>-1</sup> in RTA and  $10.3 \pm 0.7$  ml $\cdot$ min<sup>-1</sup> $\cdot$ W<sup>-1</sup> in CTRL (no significant difference). Peak  $\dot{V}O_2$  and peak work rate values are described in Table 2. As for KE, whereas the mean values of the slopes (submaximal work rates) were not different in the two

groups, the intercepts values were higher in RTA. The mean slopes of the individual regression lines were  $9.5 \pm 1.1$  ml $\cdot$ min<sup>-1</sup> $\cdot$ W<sup>-1</sup> in RTA and  $9.7 \pm 1.9$  ml $\cdot$ min<sup>-1</sup> $\cdot$ W<sup>-1</sup> in CTRL (no significant difference). Peak  $\dot{V}O_2$  and peak work rate values are described in Table 2. Peak  $\dot{V}O_2$  values normalized for muscle mass (for CE) or quadriceps muscle mass (for KE) are shown in Fig. 3.

Values of NIRS-obtained  $\Delta[\text{deoxy(Hb+Mb)}]$ , which was taken as an estimate of vastus lateralis muscle fractional O<sub>2</sub> extraction, are shown in Fig. 4 as a function of work rate during CE (left) and KE (right). Work rate intervals were defined according to the principles described above for Fig. 2. Both in RTA and CTRL, either during CE or KE, the dynamics of  $\Delta[\text{deoxy(Hb+Mb)}]$  followed a sigmoid pattern, with a tendency to plateau at  $\sim 85\%$  of peak work rate. At all work rate levels, values of  $\Delta[\text{deoxy(Hb+Mb)}]$  were significantly lower in RTA vs. CTRL, both during CE and KE; peak values were  $\sim 30\%$  lower in RTA (vs. CTRL) during either CE or KE.

ADP-stimulated mitochondrial respiration (*state 3* respiration), fueled by malate, glutamate, and succinate, as determined by high-resolution respirometry, was significantly higher (by  $\sim 60\%$ ) in RTA vs. CTRL (Fig. 5A). CS activity, taken as an estimate of mitochondrial content (24), was similar in the two groups (Fig. 5B). Maximal mitochondrial respiration induced by the chemical uncoupler FCCP, reflecting the maximal oxidative capacity of the electron transport system (ETS), was not significantly different in RTA ( $68.0 \pm 31.4$  pmol O<sub>2</sub> $\cdot$ s<sup>-1</sup> $\cdot$ mg wet wt<sup>-1</sup>) vs. CTRL ( $52.1 \pm 22.3$  pmol O<sub>2</sub> $\cdot$ s<sup>-1</sup> $\cdot$ mg wet wt<sup>-1</sup>). No differences between groups were found in “leak respiration” (Fig. 5C), reflecting the basal O<sub>2</sub> consumption not coupled to ATP synthesis, thereby suggesting that, in RTA and CTRL, the rate of “energy” dissipated by the membrane proton leak was similar. The “respiratory acceptor control ratio” (RCR), that is the ratio between *state 3* respiration and leak respiration, was taken as an index of coupling of mitochondrial respiration for a specific substrate supply (malate, glutamate, succinate in this study). A significantly higher RCR was observed in RTA vs. CTRL (Fig. 5D), suggesting a tighter coupling between oxidation and phosphorylation in RTA.

## DISCUSSION

The present study provides an integrative evaluation of oxidative metabolism in a group of young RTA characterized by a marked skeletal muscle hypertrophy. Different variables of oxidative function were evaluated, spanning from pulmonary gas exchange and skeletal muscle function in vivo to mitochondrial respiration ex vivo in permeabilized fibers. We

Table 1. Anthropometric and body composition characteristics of subjects

	RTA	CTRL
Body mass, kg	102.6 $\pm$ 7.3*	77.8 $\pm$ 6.0
Stature, m	1.84 $\pm$ 0.04	1.81 $\pm$ 0.05
BMI, kg/m <sup>2</sup>	30.1 $\pm$ 2.6*	23.8 $\pm$ 2.2
FFM, kg	90.4 $\pm$ 6.1*	66.8 $\pm$ 11.0
Body muscle mass, kg	46.1 $\pm$ 3.1*	35.2 $\pm$ 2.8
Quadriceps muscle mass, kg	3.26 $\pm$ 0.44*	2.45 $\pm$ 0.26
Body fat, %	12.2 $\pm$ 3.5*	9.9 $\pm$ 0.8

Data are means  $\pm$  SD. RTA, resistance-trained athletes; CTRL, controls; BMI, body mass index; FFM, fat-free mass. \*Significantly different from CTRL ( $P < 0.05$ ; unpaired Student's  $t$ -test).

Table 2. Peak values of investigated variables during cycle ergometer (CE) and knee-extension (KE) exercise

	CE		KE	
	RTA	CTRL	RTA	CTRL
$\dot{V}_E$ peak, (l/min)	161.6 ± 27.5	145.9 ± 28.3	69.6 ± 18.9	62.0 ± 18.0
$V_T$ peak, liters	3.2 ± 0.5*	2.7 ± 0.3	1.8 ± 0.5	1.5 ± 0.5
f peak, breaths/min	51.3 ± 8.2	55.3 ± 10.0	41.2 ± 7.4	43.8 ± 6.0
$\dot{V}_{O_{2peak}}$ , l/min	4.05 ± 0.64*	3.56 ± 0.30	1.59 ± 0.23	1.50 ± 0.33
$\dot{V}_{O_{2peak}}/BM$ , ml · min <sup>-1</sup> · kg <sup>-1</sup>	39.6 ± 5.3*	45.9 ± 3.0	—	—
$\dot{V}_{O_{2peak}}/\text{muscle mass}$ , ml · min <sup>-1</sup> · kg <sup>-1</sup>	87.9 ± 11.7*	101.5 ± 6.7	—	—
$\dot{V}_{O_{2peak}}/QM$ , ml · min <sup>-1</sup> · 100 g <sup>-1</sup>	—	—	51.5 ± 9.1*	63.7 ± 13.0
R peak	1.15 ± 0.06	1.17 ± 0.04	1.17 ± 0.14	1.13 ± 0.11
GET (% $\dot{V}_{O_{2peak}}$ )	76.7 ± 3.8	73.8 ± 4.1	78.7 ± 3.6*	72.4 ± 3.9
Work rate peak, W	314 ± 56	284 ± 15	103 ± 16	98 ± 13
Time to exhaustion, min	15.7 ± 2.8	14.2 ± 0.7	14.3 ± 2.2	13.5 ± 1.7
HR peak, beats/min	184 ± 8	186 ± 11	142 ± 13	146 ± 11
Q peak, l/min	29.1 ± 3.9	27.2 ± 2.8	18.9 ± 4.5	17.9 ± 3.2
CI peak, liter · min <sup>-1</sup> · m <sup>-2</sup>	12.8 ± 1.6	13.7 ± 1.4	8.3 ± 1.9	9.1 ± 1.4

Data are expressed as means ± SD.  $\dot{V}_E$ , pulmonary ventilation;  $V_T$ , tidal volume; f, respiratory frequency;  $\dot{V}_{O_{2peak}}/BM$ , oxygen uptake per unit of body mass;  $\dot{V}_{O_{2peak}}/\text{muscle mass}$ , oxygen uptake per unit of whole body muscle mass; R, gas exchange ratio; GET, gas exchange threshold; HR, heart rate; Q, cardiac output; CI, cardiac index. See text for further details. \*Significantly different from CTRL ( $P < 0.05$ ; unpaired Student's *t*-test).

hypothesized, in RTA vs. CTRL, an impaired oxidative function in vivo and an impaired mitochondrial respiratory function ex vivo. The obtained results did not confirm these hypotheses.

Whole body peak oxidative function was enhanced in RTA vs. CTRL. Figure 2 (left), in which pulmonary  $\dot{V}_{O_2}$  data are expressed in liters per minute shows that, during CE,  $\dot{V}_{O_{2peak}}$  was indeed higher (by ~15%) in RTA vs. CTRL, in association with a slightly higher (by ~10%) peak work rate. Moreover, despite the significantly greater body mass, during CE, no impairment of oxidative function was seen in RTA at submaximal work rates: the efficiency and the “O<sub>2</sub> cost” of exercise (as indicated by the slopes and the intercepts of the  $\dot{V}_{O_2}$  vs. work rate relationships) were indeed the same in the two groups. This finding is of interest, also compared with what is usually seen in another population characterized by a significantly greater body mass, such as obese patients, in which the  $\dot{V}_{O_2}$  vs. work rate relationship is shifted upward compared with that seen in normal controls (22), indicating a higher O<sub>2</sub> cost of CE exercise deriving from the excess in body mass.

The situation was in part different for KE (Fig. 2, right): the slopes of the  $\dot{V}_{O_2}$  vs. submaximal work rates relationships were again similar in the two groups, but the intercept was higher in RTA (suggesting a higher O<sub>2</sub> cost for KE exercise), and  $\dot{V}_{O_{2peak}}$  and peak work rate values were only slightly higher in RTA. No clear-cut explanation can be given for the higher O<sub>2</sub> cost of exercise observed in RTA during KE but not during CE. Cardiovascular constraints cannot be hypothesized, since they were by definition much lower in KE vs. CE. It can be hypothesized that the work of accessory muscles (see Ref. 34) during KE was overall higher in RTA vs. CTRL. We indeed measured pulmonary  $\dot{V}_{O_2}$  and not  $\dot{V}_{O_2}$  across the leg, and as a consequence of this we cannot discriminate between  $\dot{V}_{O_2}$  attributable to the legs and  $\dot{V}_{O_2}$  attributable to the rest of the body.

On the other hand, after we normalized  $\dot{V}_{O_{2peak}}$  per whole body muscle mass (for CE) or quadriceps muscle mass (for KE), values were significantly lower (by ~15–20%) in RTA vs. CTRL (see Fig. 3). This finding could be interpreted from

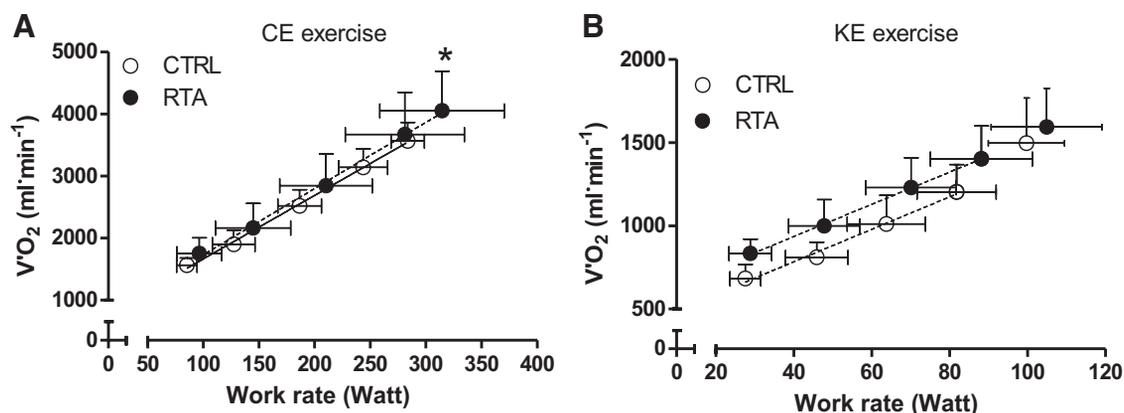
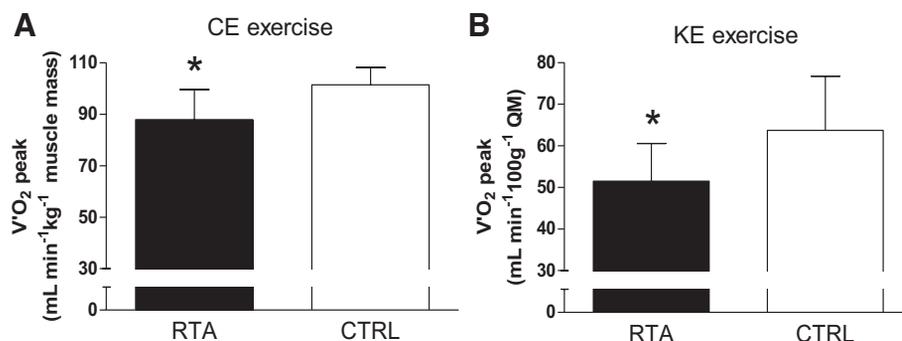


Fig. 2. Means ± SD  $\dot{V}_{O_2}$  values during CE (A) and knee extension (KE; B) are plotted as a function of means ± SD work rate (Watt) for RTA and CTRL. Individual  $\dot{V}_{O_2}$  values were grouped for discrete work rate intervals. As for CE, the means ± SD values of the slopes of the individual regression lines were  $10.6 \pm 0.9$  ml·min<sup>-1</sup>·W<sup>-1</sup> in RTA and  $10.3 \pm 0.7$  ml·min<sup>-1</sup>·W<sup>-1</sup> in CTRL (not significant); the mean values of the intercepts were  $652 \pm 96$  ml/min in RTA and  $613 \pm 83$  ml/min in CTRL (not significant). As for KE, the mean values of the slopes of the individual regression lines (submaximal work rates) were  $9.5 \pm 1.1$  ml·min<sup>-1</sup>·W<sup>-1</sup> in RTA and  $9.7 \pm 1.9$  ml·min<sup>-1</sup>·W<sup>-1</sup> in CTRL (not significant); the mean values of the intercepts were  $545 \pm 71$  ml/min in RTA and  $421 \pm 81$  ml/min in CTRL ( $P < 0.05$ ). \*Significant difference vs. CTRL ( $P < 0.05$ ). See text for further details.

Fig. 3. Peak  $\dot{V}O_2$  values normalized for whole body muscle mass during CE (A) or quadriceps muscle mass during KE (B) in RTA vs. CTRL. \*Significant difference vs. CTRL ( $P < 0.05$ ).



two different perspectives: despite a lower  $\dot{V}O_{2\text{peak}}$  per unit muscle mass, RTA reached slightly higher (during CE) or similar (during KE) peak work rate levels than CTRL, suggesting a higher muscle/metabolic efficiency (see below). On the other hand, it should also be recognized that  $\dot{V}O_{2\text{peak}}$ /muscle mass was substantially lower in RTA, suggesting a substantial impairment of peak oxidative function *in vivo* when normalized for the markedly greater muscle mass. Or, to put it in other words, in RTA (vs. CTRL), the increase in muscle mass was more pronounced than the increase in maximal oxidative power.

How to interpret all these findings in a reasonably coherent scenario? The answer may come both from some literature data and from data obtained in the present study.

First of all, strength training may have positive effects on aerobic performance and muscle oxidative metabolism. In the present study, RTA had greater maximal isometric force vs. CTRL. For the same force (and power) output, muscles with higher maximal force would need to recruit a lower number of motor units and, therefore, more oxidative (and more efficient) muscle fibers (20, 26). Previous literature data confirm that strength training may increase skeletal muscle efficiency (4) and enhance skeletal muscle “metabolic stability” (50). This would also be in agreement with our high-resolution respirometry data, suggesting an enhanced mitochondrial respiratory function in RTA (see below).

On the other hand, the marked muscle hypertrophy per se could impair the peripheral diffusion of  $O_2$  if it is not accompanied by a proportional increase in muscle capillary supply. In the present study, quadriceps muscle mass and CSA were ~35% greater in RTA than in CTRL. It is generally assumed that the increase in muscle mass and size obtained by resistance

training is mainly determined by hypertrophic processes involving single muscle fibers (12). According to Aagaard et al. (1), in the hypertrophic muscle, the increase of CSA of individual fibers is more pronounced (by ~6%) to that observed for the muscle as a whole, as a consequence of changes in the pennation angle of fibers within the muscle. Thus CSA of individual fibers in the RTA of the present study could have been 40–45% greater than that of CTRL, possibly representing an important impediment to muscle  $O_2$  diffusing capacity (see below). Muscle capillary supply was not determined in the present study, and literature data are not univocal. According to some authors, skeletal muscle hypertrophy induced by strength training could determine a capillary “dilution” in the tissue (43). A lower microvascular surface area available for gas exchange and/or an increased diffusion distance from the capillary to mitochondria would impair peripheral  $O_2$  diffusion (46). In the present study, we did not determine muscle capillarity or peripheral  $O_2$  diffusion; the latter could be determined by the invasive method developed in Dr. Wagner’s laboratory over the years (e.g., see Ref. 46). These approaches could be attempted in future studies. In the hypertrophic skeletal muscles, also an altered matching between  $O_2$  delivery and  $O_2$  utilization within the muscles could lead to the lower muscle  $O_2$  availability.

Evidence in favor of this phenomenon is provided, in the present study, by the observation in RTA of lower fractional  $O_2$  extraction values, both at submaximal and at peak work rates during both CE and KE (Fig. 4). As nicely discussed by Poole et al. (31), it would be an oversimplification to interpret fractional  $O_2$  extraction simply as a result of “muscle factors”; indeed, this variable may be affected by a combination of interrelated factors responsible for perfusive  $O_2$  transport to

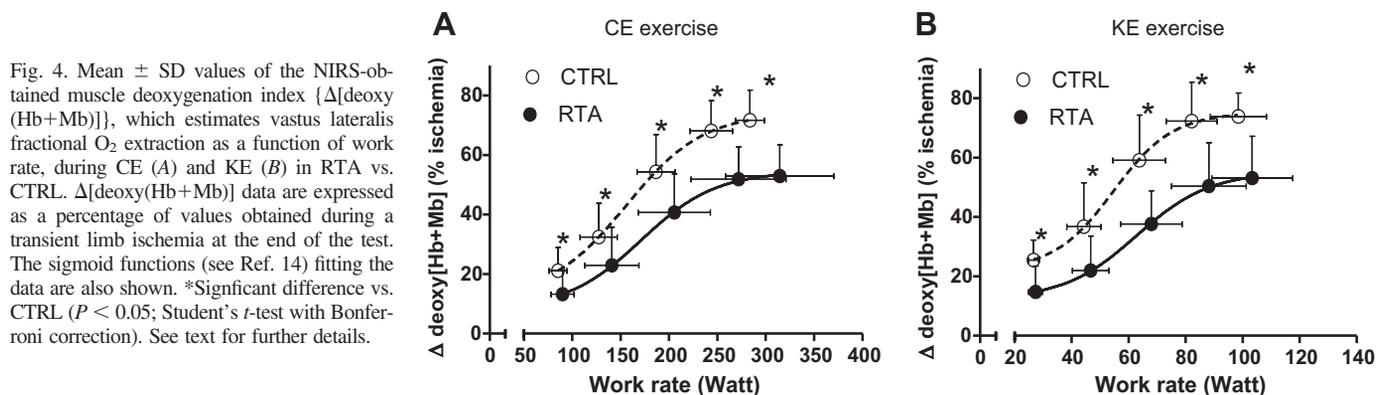


Fig. 4. Mean  $\pm$  SD values of the NIRS-obtained muscle deoxygenation index  $\{\Delta[\text{deoxy}(\text{Hb}+\text{Mb})]\}$ , which estimates vastus lateralis fractional  $O_2$  extraction as a function of work rate, during CE (A) and KE (B) in RTA vs. CTRL.  $\Delta[\text{deoxy}(\text{Hb}+\text{Mb})]$  data are expressed as a percentage of values obtained during a transient limb ischemia at the end of the test. The sigmoid functions (see Ref. 14) fitting the data are also shown. \*Significant difference vs. CTRL ( $P < 0.05$ ; Student’s *t*-test with Bonferroni correction). See text for further details.

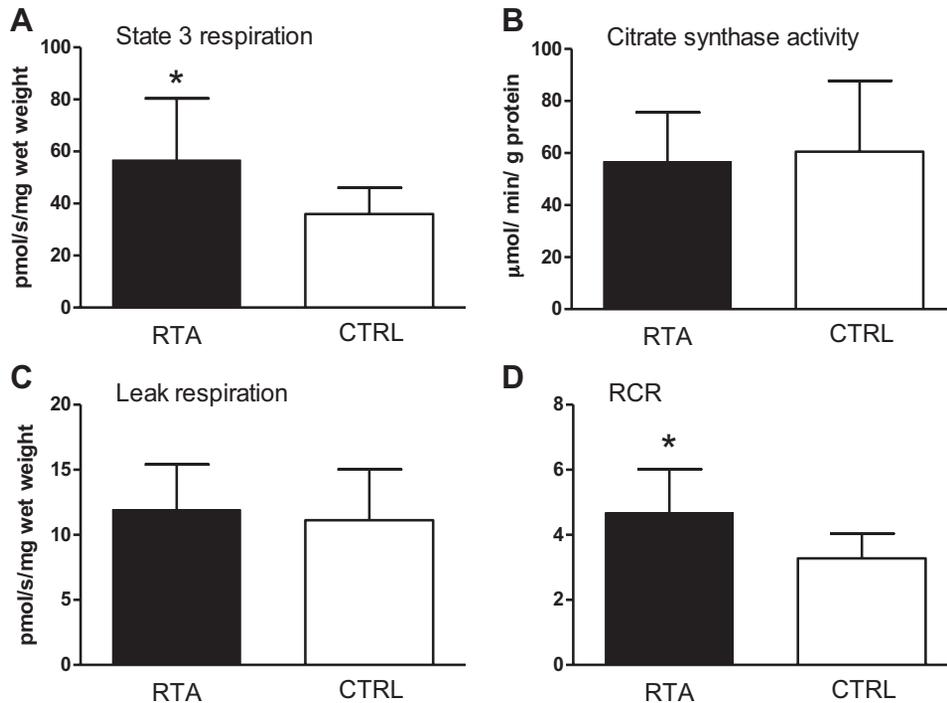


Fig. 5. Mean  $\pm$  SD values of mitochondrial *state 3* respiration (with glutamate, malate, and succinate as substrates) per unit tissue mass (wet weight) measured in permeabilized muscle fibers (A), and citrate synthase activity (in  $\mu\text{mol}\cdot\text{min}^{-1}\cdot\text{g}^{-1}$  protein; B) in RTA and CTRL. Mean  $\pm$  SD values of leak respiration (respiratory rate in the presence of substrates without ADP; C) and respiratory acceptor control ratio (RCR; *state 3* respiration/leak respiration; D), denoting the degree of coupling of mitochondrial respiration in RTA and CTRL. \*Significant difference vs. CTRL ( $P < 0.05$ ). See text for further details.

and within active muscles and diffusive  $\text{O}_2$  transport within fibers. In the present study, however, the lower  $\text{O}_2$  extraction cannot be accounted for by cardiovascular  $\text{O}_2$  delivery (the impaired  $\text{O}_2$  extraction was described both during CE and KE, in which, by definition, cardiovascular constraints are reduced or eliminated) or by an impaired mitochondrial respiratory function, which was enhanced, at least in *ex vivo* conditions, in RTA vs. CTRL. Thus the “bottleneck” of oxidative metabolism in RTA would reside “downstream” of bulk cardiovascular  $\text{O}_2$  delivery but “upstream” of intracellular oxidative metabolism. The main impairment could then reside in the diffusing capacity of the muscle for  $\text{O}_2$  and/or in the intramuscular matching between  $\text{O}_2$  delivery and  $\text{O}_2$  utilization, which could be altered as a consequence of the marked muscle hypertrophy.

By measures of high-resolution respirometry carried out in permeabilized skeletal muscle fibers (experimental conditions of unlimiting  $\text{O}_2$  availability), we indeed observed higher values of ADP-stimulated mitochondrial respiration in RTA vs. CTRL, associated with a higher degree of coupling between oxidation and phosphorylation. These observations suggest an enhanced *ex vivo* respiratory function in RTA. These data were obtained in the presence of a similar CS activity in the two groups. Although the method has some limitations (see Ref. 24), the activity of the enzyme is frequently utilized to estimate mitochondrial content. Thus, in the markedly hypertrophic skeletal muscles of RTA, mitochondrial biogenesis occurred proportionally to contractile protein synthesis. The finding appears consistent with studies on molecular signaling showing that the mammalian target of rapamycin (mTOR) kinase, which is known to be activated by resistance training and to be involved in the signaling pathway of protein synthesis and muscle growth, also regulates the expression of mitochondrial genes and may have a critical regulatory role on mitochondrial biogenesis and function (38, 47). *State 3* mitochondrial respiration was higher in RTA vs. CTRL, whereas no differences

were described between the two groups in terms of leak respiration. These data suggest a tighter coupling of mitochondrial respiration and an improved efficiency of the phosphorylation system in RTA. Similar findings have been observed by other authors after long-term exercise training (44, 51), in association with a more efficient control of mitochondrial respiration by the creatine kinase system. These adaptations are expected to limit perturbations of cellular homeostasis during exercise and to delay the increased reliance on substrate level phosphorylation for ATP regeneration, thus preserving exercise tolerance (51), and are likely associated with the concept of muscle “metabolic stability” (49).

Which could be the cause(s) responsible for the improved mitochondrial respiratory function *ex vivo* in RTA? Apart from the direct effects of training, it can be hypothesized that the impaired peripheral  $\text{O}_2$  diffusing capacity and/or the impaired matching between  $\text{O}_2$  delivery and  $\text{O}_2$  utilization, discussed above, could determine within the exercising hypertrophic muscles areas of relative lack of  $\text{O}_2$ , that is of hypoxia. An improved coupling of mitochondrial respiration could then result from adaptive responses of mitochondria to repeated hypoxic stimuli. In skeletal muscle, a hypoxia-sensitive signal activation of transcription may occur in the myocellular compartment as a direct consequence of a drop in tissue oxygenation to maintain the homeostasis of  $\text{P}_{\text{O}_2}$  at the levels considered critical for the function of cell (11). The multi-gene hypoxia-inducible transcription factor (HIF)-1 is recognized as the master transcription regulator of cell hypoxic signaling (39). HIF-1 drives the expression of a variety of genes involved in mitochondrial metabolism in skeletal muscle under hypoxic exposure, among which are those controlling the efficiency of cytochrome *c* oxidase enzyme (COX) in the mitochondrial respiratory chain. HIF-1 would coordinate a switch from COX4-1 subunit to COX4-2, thereby increasing the efficiency of electron transfer to  $\text{O}_2$  at complex IV and minimizing

electron leakage at complexes I and III. This switch would also enhance the efficiency of ATP synthesis by increasing proton pumping into the mitochondrial intermembrane space (16). By this way, electron transfer and phosphorylation would be more tightly coupled, and the efficiency of oxidative phosphorylation would be improved.

### Methodological Considerations

In the present study, the values of ADP-stimulated mitochondrial respiration and maximal uncoupled respiration were in the low end of values for healthy subjects' quadriceps muscles. A wide range of values for mitochondrial respiratory capacity can be found in the literature (17). This could be attributable to the investigated population, to intrinsic metabolic characteristics of tissue samples, and to methodological procedures, such as titration protocol, sequence, and combination of administered substrates, [ADP], experimental temperature, wet or dry state of tissue mass utilized for normalization, fresh or frozen tissue samples, etc. (17). In any case, the data obtained in the present study are similar to those obtained after substantially following the same protocol of the present study in the healthy control subjects of recent studies (9, 23, 30). In the present study, after adding cytochrome *c* to the measuring chamber, the increase in mitochondrial respiration was very small (~2%). A small increase in respiration after adding cytochrome *c* is a standard criterion to check the absence of significant damage of the outer mitochondrial membrane, possibly occurring during the preparation of samples.

At first sight a comparison of  $\dot{V}O_2$  between the two groups at submaximal work rates may not be warranted since the two groups presumably have different  $\dot{V}O_2$  kinetics (slower in RTA), and as a consequence different rates of adjustment to the work rate increments. However, as elegantly discussed in the recent review by Rossiter (35), during a standard incremental test, different time constants of the  $\dot{V}O_2$  kinetics do not affect the slope of the  $\dot{V}O_2$  vs. work rate relationship but only shift the linear relationship to the right (in case of slower  $\dot{V}O_2$  kinetics) or to the left (in case of faster  $\dot{V}O_2$  kinetics), the "horizontal distance" between these linear relationships being reflected by the difference in time constants. We did not determine the  $\dot{V}O_2$  kinetics in the two groups of subjects of our study. However, if we assume slower  $\dot{V}O_2$  kinetics in the strength-trained group, imagine a difference in time constants of 15 s (this is likely an exaggeration, considering that both groups had a common endurance training background), and assume the same gain in the two groups (as actually observed in this study), the small horizontal shifts of the  $\dot{V}O_2$  vs. work rate relationships do not change data interpretation: same slopes and intercepts between the two groups during CE and same slopes but higher intercepts in RTA during KE, suggesting a slightly higher  $O_2$  cost of KE exercise in this group.

In conclusion, in a group of young RTA characterized by a marked skeletal muscle hypertrophy, the greater muscle mass and maximal force and the enhanced mitochondrial respiratory function seem to compensate for the hypertrophy-induced impaired peripheral  $O_2$  diffusion. The net results are an enhanced whole body oxidative function at peak exercise and unchanged efficiency and  $O_2$  cost at submaximal exercise, despite the much greater muscle mass and body mass.

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### DISCLOSURES

No conflicts of interest, financial or otherwise, are declared by the author(s).

### AUTHOR CONTRIBUTIONS

Author contributions: D.S., R.D., S.L., S.P., J.R., and B.S. performed experiments; D.S. and G.R. analyzed data; D.S., I.M., and B.G. interpreted results of experiments; D.S. prepared figures; D.S. and B.G. drafted manuscript; D.S., R.D., S.L., S.P., J.R., G.R., I.M., B.S., R.P., and B.G. edited and revised manuscript; D.S., R.D., S.L., S.P., J.R., G.R., I.M., B.S., R.P., and B.G. approved final version of manuscript; R.P. and B.G. conception and design of research.

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